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A Biomagentic fluid dynamic model for the MHD Couette Flow between two infinite horizontal parallel Porous plates

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Abstract

A model of biomagentic fluid dynamics, which is suitable for the description of the MHD Couette flow of a viscous-incompressible fluid, is discussed in this work. Here we take two infinite horizontal parallel porous flat plates. The upper plate is subjected to a constant suction while the lower plate is to a transverse sinusoidal injection along with the velocity distribution. In this work finite difference method is used for solving the non-linear partial differential equations and our results shows that the main flow component (U) decreases with the increase of Hartmann number (M) and the velocity decreases with the increases of the injection suction parameter (R). Here we also investigate the effects of Hartmann number (M) and suction parameter (R) along with the velocity and temperature distribution.

Key words: Hartmann number, Prandtl number, permeability parameter, suction parameter, Grashof number.

AMS Subject Classification: 76z05

1. Introduction

The steady flow of an electrically conducting fluid has many applications in biological and engineering problems such as magnetohydrodynamics (MHD) generators, plasma studies, nuclear reactors, geothermal energy extraction, the boundary layer control in the field of aerodynamics, blood flow problems, petroleum technology to steady the movement of natural gas, and in oil and water industries through the oil channel etc.

Gersten and Gross[1] studied on the

three dimensional convective flow and heat transfer through a porous medium, while Raptis[2] worked on the free convective flow through a porous medium bonded by the infinite vertical plate with oscillating plate temperature and constant suction, and again Raptis and Perdikis[3] further worked on the free convective flow through a highly porous medium bounded by the infinite vertical porous plate with constant suction. Although in above studies the investigators have restricted themselves to two-dimensional flows, but there may arise situations, where the flow field may be essentially three-dimensional. Therefore Singh[4] worked on three dimensional MHD flow past a porous plate, while Mazumdar *et al*.[5] discussed about some effects of magnetic field on flow of a newtonian fluid through a circular tube.

Ahmed and Sharma[6] discussed about the three-dimensional free convective flow of an incompressible viscous fluid through a porous medium with uniform free steam velocity, while Singh[7] again studied about a three-dimensional couette flow with transpiration cooling by applying transverse sinusoidal injection velocity at the stationary plate velocity. Kim[8] discussed the unsteady MHD convective heat transfer past a semi-infinite vertical porous moving plate with variable suction, and Kamel[9] discussed about the unsteady MHD convection through porous medium with combined heat and mass transfer with heat source/sink. Amos and Ogulu[10] studied the magnetic effect on pulsatile flow in a constricted axissymmetric tube. Kumar *et al*.[11] discussed about the hall current on MHD free-convection flow through porous media past a semi-infinite vertical plate with mass transfer, while Muhammad and Hayat[12] worked on the effects of hall current and heat transfer on flow due to a pull of eccentric rotating. Attia[13] observed the unsteady MHD couette flow and heat transfer of dusty fluid with variable physical properties, while Kumar and Kumar[14] discussed about the numerical steady of the axisymmetric blood flow in a constricted rigid tube. The effects of magnetic field and body acceleration on axial velocity of pulsatile blood flow in inclined circular tube have been discussed graphically by Sanyal *et al*.[15]. Again Rathod and Tanveer[16] worked on the pulsatile flow of blood through a porous medium under the effect of magnetic field by considering blood as couple stress fluid through a straight and rigid circular tube using Laplace and finite Hankel transform. Mishra and Verma[17] discussed the effect of stenosis on non Newtonian blood flow through uniform or non-uniform cross-section of blood vessels, while a two-phase non-linear model for blood flow in asymmetric and axisymmetric stenosed arteries were designed by Sankar[18].

The main purpose of this work is to analyze the effects of electrically conducting three dimensional, viscous incompressible fluid between two porous plate with the observation of the velocity and temperature distribution along with the effects of Hartmann number (M) and suction parameter (R).

2. Mathematical Analysis:

A three dimensional flow of a viscous incompressible fluid through a porous medium, which is bounded by a vertical infinite porous plate is considered. The coordinate system with plate lying vertically on X-Z plane, where upper plate is at distant *a* apart such that X- axis is taken along the plate in the direction of the plane and Y- axis is perpendicular to the plane. The lower and upper plate's temperature considered to be T_0 and T_1 respectively with ($T_1>T_0$) and the upper plate is subjected to a constant velocity U along X- axis, while the lower plate to a transverse sinusoidal injection velocity of the following forms:

$$V\left(z\right)=v\left(1+\varepsilon\cos\frac{\pi z}{a}\right) \qquad \text{(i)}$$

Now denoting the velocity component v_1, v_2, v_3 in the x, y and z direction respectively and temperature by T, then problem is governed by the following equations.

Continuity equation:

$$\frac{\partial v_2}{\partial y}+\frac{\partial v_3}{\partial z}=0 \qquad \text{(ii)}$$

Momentum equations:

$$v_2\frac{\partial v_1}{\partial y}+v_3\frac{\partial v_1}{\partial z}=\nu\left(\frac{\partial^2 v_1}{\partial y}+\frac{\partial v_1}{\partial z}\right)+g\beta(T_0-T_1)-\sigma\frac{\beta_0^2 v_1}{\rho} \qquad \text{(iii)}$$

$$v_2\frac{\partial v_2}{\partial y}+v_3\frac{\partial v_2}{\partial z}=-\frac{1}{\rho}\frac{\partial p}{\partial y}+\nu\left(\frac{\partial^2 v_2}{\partial y^2}+\frac{\partial^2 v_2}{\partial z^2}\right)-\frac{\nu}{k}v_2 \qquad \text{(iv)}$$

$$v_2\frac{\partial v_3}{\partial y}+v_3\frac{\partial v_3}{\partial z}=-\frac{1}{\rho}\frac{\partial p}{\partial z}+\nu\left(\frac{\partial^2 v_3}{\partial y^2}+\frac{\partial^2 v_3}{\partial z^2}\right)-\frac{\sigma\beta_0^2 v_3}{\rho} \qquad \text{(v)}$$

and the energy equation is

$$v_2\frac{\partial T}{\partial y}+v_3\frac{\partial T}{\partial z}=\alpha\left(\frac{\partial^2 T}{\partial y^2}+\frac{\partial^2 T}{\partial z^2}\right) \qquad \text{(vi)}$$

while the boundary conditions of this modal are

$$\left.\begin{array}{llll}\text{at } y=0,\ v_1=0, & v_2(z)=v\left(1+\varepsilon\cos\dfrac{\pi z}{a}\right), & v_3=0, & T=T_0\\ \text{at } y=a,\ v_1=U, & v_2=v, & v_3=0, & T=T_1\end{array}\right\} \qquad \text{(vii)}$$

Now we introduce following non-dimensional variables, which change the governing equations in the dimensionless form

$$\left.y'=\frac{y}{a},\quad z'=\frac{z}{a},\quad u=\frac{v_1}{U},\quad v=\frac{v_2}{v},\ w=\frac{v_3}{v},\quad p=\frac{P}{\rho v^{2,}},\quad \theta=\frac{T-T_0}{T_1-T_0}\right\} \qquad \text{(viii)}$$

In this model we use some special numbers/ parameters, which are along with their notations as follows:

Suction parameter $(R)=\frac{av}{\nu}$, Hartmann number $(M)=\frac{\beta_0}{V}\sqrt{\frac{\sigma}{\mu}}$,

Prandtl number $(P_r)=\frac{\nu}{\alpha}$, Grashof number $(G_r)=\frac{g\beta\rho^2(T_0-T_1)}{\mu^2}a^3$,

where β_0-magnetic field component along Y-axis, k- permeability of the porous medium, U-velocity along X-axis, α - thermal diffusivity, β - volumetric coefficient of the thermal expansion, ρ - density of fluid, ν - kinematics viscosity, μ - viscosity and θ - temperature.

Here in the light of (viii) the boundary conditions (vii) and the governing equations (ii) to (vi), becomes in the following form:

$$\frac{\partial v}{\partial y}+\frac{\partial w}{\partial z}=0 \qquad \text{(ix)}$$

$$v\frac{\partial u}{\partial y}+w\frac{\partial u}{\partial z}=\frac{1}{R}\left(\frac{\partial^2 u}{\partial y^2}+\frac{\partial^2 u}{\partial z^2}\right)+\frac{G_r\nu}{aRU}-\frac{M^2 u}{R} \qquad \text{(x)}$$

$$v\frac{\partial v}{\partial y}+w\frac{\partial v}{\partial z}=-\frac{\partial P}{\partial y}+\frac{1}{R}\left(\frac{\partial^2 v}{\partial y^2}+\frac{\partial^2 v}{\partial z^2}\right)-\frac{a^2 v}{Rk} \qquad \text{(xi)}$$

$$v\frac{\partial w}{\partial y}+w\frac{\partial w}{\partial z}=-\frac{\partial P}{\partial z}+\frac{1}{R}\left(\frac{\partial^2 w}{\partial y^2}+\frac{\partial^2 w}{\partial z}\right) \qquad \text{(xii)}$$

$$v\frac{\partial \theta}{\partial y}+w\frac{\partial \theta}{\partial z}=\frac{1}{RP_r}\left(\frac{\partial^2 \theta}{\partial y^2}+\frac{\partial^2 \theta}{\partial z^2}\right) \qquad \text{(xiii)}$$

3. *Numerical Solution:*

In this model we apply the finite difference method to solve the governing non-linear equations. by transforming the first and second order derivatives by using the forward and central differences formulas. Here i, j represent the moment along Y and Z direction respectively, and let, there is a square mesh ($\Delta y=\Delta z=h$), then the equations (ix) to (xiii) along with the boundary conditions are as:

$$u_{i,j+1}=\frac{1}{\left(Rhw_{i,j}-1\right)}\left[\left(1-Rhv_{i,j}\right)u_{i+1,j}+\left\{Rh\left(v_{i,j}+w_{i,j}\right)-\left(4+M^2h^2\right)\right\}u_{i,j}+\left(u_{i-1,j}+u_{i,j-1}\right)+\frac{\nu hG_r}{aRU}\right] \qquad \text{(xiv)}$$

$$v_{i,j+1}=\frac{1}{\left(Rhwv_{i,j-1}\right)}\left[\left(1-Rhv_{i,j}\right)v_{i+1,j}+\left\{Rh\left(v_{i,j}+w_{i,j}\right)-\left(4+\frac{a^2h^2}{K}\right)\right\}v_{i,j}+\left(v_{i-1,j}+v_{i,j-1}\right)++Rh\Delta P\right] \qquad \text{(xv)}$$

$$w_{i,j+1}=\frac{1}{\left(Rhw_{i,j}-1\right)}\left[\left(1-Rhv_{i,j}\right)w_{i+1,j}+\left\{Rh\left(v_{i,j}+w_{i,j}\right)-\left(4+M^2h^2\right)\right\}w_{i,j}+Rh\Delta P\right] \qquad \text{(xvi)}$$

and temperature equation

$$\theta_{i,j+1}=\frac{1}{\left(RhP_r w_{i,j}-1\right)}\left[\left(1-RhP_r v_{i,j}\right)\theta_{i+1,j}+\left\{RhP_r\left(v_{i,j}+w_{i,j}\right)-4\right\}\theta_{i,j}+\left(\theta_{i-1,j}+\theta_{i,j-1}\right)\right] \qquad \text{(xvii)}$$

4. Results and Discussion

The main flow velocity component u, applied through the porous plate at rest, due to the transverse sinusoidal injection velocity is obtained from equation (xiv). We described the fig-(a) from the equation (xiv) which shows the flow component u decreases with the increase of Hartmann number M, injection parameter R and permeability k of the porous medium.

Fig. (a) Main flow velocity profile for z=0

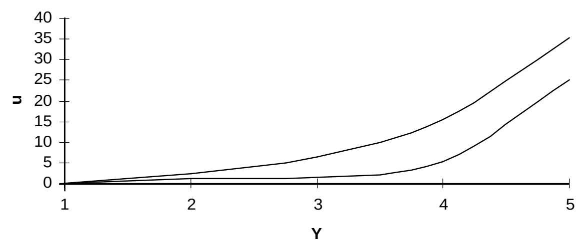


Fig.(b) Main flow velocity profile for z=0.5

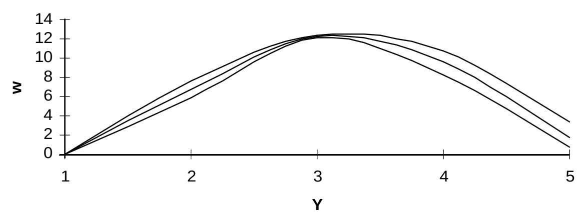
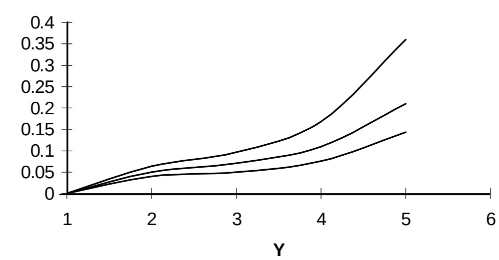


fig. (c) Temperature distribution



We described velocity profile for the small and large value of permeability of the porous medium through the fig.-(b), which shows the velocity decrease with the increase of the injection suction parameter R, it is also observed that increase in the permeability of the porous lead to an increase in the flow velocities.

The fig(c) shows that the rate of heat transfer coefficient at the stationary porous plate. In this case the values of Prandtl number Pr are chosen as 0.5 approximately, which represents air and water at 15ºC. Here it is found that the rate of heat transfer is much lower in the case of water than in air.

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